Safety of poly (ethylene glycol)-coated perfluorodecalin-filled poly (lactide-co-glycolide) microcapsules following intravenous administration of high amounts in rats

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1. Introduction

Artificial blood substitutes are urgently needed to guarantee the rising blood supply of the population. Packed red cells are inadequately available, require cold storage conditions, display a short shelf-life and are associated with problems such as blood group compatibility and risk of transmission of various diseases [1]. Thus, alternatives such as perfluorocarbon-based oxygen carriers have moved into the focus of medical research. Perfluorocarbons (PFCs) are fluorinated hydrocarbons dissolving effectively the main respiratory gases oxygen and carbon dioxide in a manner that depends linearly on the partial pressure of the correspondent gas [2]. Their known chemical and biological inertness, due to the strength of the carbon-fluorine bonds, make them perfect candidates for medical applications but also evoke galenical problems [2]. So far, PFCs were always engineered as oil-in-water emulsions (in which PFC constitutes the oil phase) rendering them blood-compatible for intravenous administration [1]. However, typical problems such as biological incompatibility of the used emulsifiers, coalescence and flocculation of emulsion droplets leading to an increased particle size could not be satisfactorily eliminated [3]. We tried to overcome these problems by engineering biocompatible poly (ethylene glycol)-coated poly (l-lactide-co-glycolide) microcapsules (PLGA microcapsules) with a PFC core [4,5]. PLGA and poly (ethylene glycol) (PEG) are metabolizable, harmless compounds, that are approved by the Food and Drug

Abbreviations: ALAT, alanine aminotransferase; ANOVA, one-way analysis of variance; ASAT, aspartate aminotransferase; BE, base excess; CARPA, complement activation-related pseudoallergy; CK, creatine kinase; C3, complement factor 3; variance; ASAT, aspartate aminotransferase; BE, base excess; CARPA, complement activation-related pseudoallergy; CK, creatine kinase; C3, complement factor 3; C4a, complement factor 4a; DAPI, 4',6-diamidin-2-phenylindol; FITC-dextran, fluorescein isothiocyanate-dextran 150,000; IFN-γ, interferon-gamma; IL, interleukin; IVM, intravitreal microscopy; LDH, lactate dehydrogenase; MAP, mean arterial blood pressure; PEG, poly (ethylene glycol); PFD, perfluorodecalin; PLGA, poly (l-lactide-co-glycolide); PVA, poly (vinyl alcohol); TFN-α, tumor necrosis factor alpha

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Administration for internal use in humans, thus representing ideal raw materials for the design of intravenously applicable drug carriers [5]. To our knowledge, in vivo data are missing about intravenously administered microparticles made of PEG and PLGA, although these two materials are very common substances that have been excessively explored. Moreover, there generally exist only very few in vivo data about microparticles designed for intravenous application [6,7]. Certainly this is because the design of microcarrier systems for intravascular use represents a special challenge [7]. In difference to ultrasonic contrast agents or usual drug carriers, the dedication of microparticles as artificial oxygen carriers requires the safe intravenous application of very high amounts of the pharmaceutical [10].

The principal suitability of PFCs as artificial oxygen carrier is widely recognized in the literature [19] and the general feasibility of intravenous administration of our PFD-filled PLGA microcapsules has already been demonstrated [5]. Favorably, the pharmaceutical agent PFD must only be encapsulated and the intact capsule wall must allow an effective gas exchange. In the present work we focused on the detailed investigation of side effects caused by the intravenous administration of very high amounts of PFD-filled PLGA microparticles in further use as artificial oxygen carriers, because until now, none of the current formulations of hemoglobin-based or perfluorocarbon-based artificial oxygen carriers can be infused without toxic effects in sufficient amounts in order to preserve aerobic metabolism in all tissues [10].

2. Materials

2.1. Chemicals

Poly (ε,ε-lactide-co-glycolide) (PLGA) (50:50) produced by LACTEL (86013-2P, inherent viscosity in chloroform 0.67 dl/g) was purchased from NRC Nordmann Rassmann (Hamburg, Germany). Poly (ε,ε-lactide-co-glycolide) (50:50) copolymers covalently attached with poly (ethylene glycol) (PEG) (RESOMER PEG Sample CR, RGPD50155, inherent viscosity in chloroform 0.50 dl/g) were obtained from Boehringer Ingelheim (Ingelheim, Germany). Nile red, fluorescein isothiocyanate-dextran 150,000 (FITC-dextran) and poly (vinyl alcohol) (PVA, Mw 9000 – 10,000, 80% hydrolyzed) came from Sigma (Deisenhofen, Germany). Perfluorodecalin (PFD) was from F2 Chemicals (Preston, United Kingdom). Isoflurane (Forene®) was obtained from Abbott (Wiesbaden, Germany), ketamine 10% from Ceva (Düsseldorf, Germany) and lidocaine (Xylocain® 1%) from AstraZeneca (Wedel, Germany). Portex® catheters (0.58 mm i.d./0.96 mm o.d.) were purchased from Smiths Medical International (Hythe, United Kingdom). Medical oxygen was obtained from Air Liquide (Düsseldorf, Germany), ringer solution from Fresenius (Bad Homburg, Germany) and sterile NaCl 0.9% Ecolflac from B. Braun, Melsungen, Germany. Paraffin (Paraplast Tissue Embedding Medium REF 501,006) was from McCormick Scientific (St. Louis, USA). Cryomatrix (Shandon Cryomatrix) was purchased from Thermo, Fisher Scientific (Waltham, USA) and Mounting Medium (Vectashield Hard Set Mounting Medium with DAPI, H-1500) from Vector Laboratories (Burlingame, USA).

3. Methods

3.1. Capsule preparation

PFD-filled PEG-PLGA microcapsules (diameter of 1.5 ± 0.8 μm) were prepared by an emulsion-evaporation procedure as described before [5]. Briefly, an organic solution of 100 mg PLGA (92% PLGA, 8% PEG-PLGA) and 100 μl PFD in 6 ml methylene chloride was emulsified into 20 ml of an aqueous solution of 1% PVA by using an Ultraturrax T25 (IKA Werke, Staufen, Germany) operating with an S25KV-25G-IL dispersing tool at a velocity of 10,200 rpm. For preparation of PEG-PLGA microspheres (unfilled polymer particles with a diameter of 1.5 ± 0.8 μm) Ultraturrax velocity was changed to 5400 rpm. The used methylene chloride was evaporated under magnetic stirring. Microcapsules (independent of the capsule type) were centrifuged (199.6 g, 20 min, Biofuge primo R, Heraeus, Hanau, Germany) and washed three times with sterile 0.9% NaCl. The final pellet was resuspended in 10 ml sterile 0.9% NaCl and subsequently filtered using a 2.7 μm pore size syringe filter (Whatman, Dassel, Germany). For the preparation of PFD-filled PEG-PLGA microcapsules with a lower preparation of PFD-filled PEG-PLGA microcapsules with a lower size of 1 ± 0.5 μm, Ultraturrax velocity was changed to 14,000 rpm and a 1.6 μm pore size syringe filter (Whatman, Dassel, Germany) was used as described previously [11].

For evaluating frozen sections of various organs after contact with PFD-filled PEG-PLGA microcapsules (diameter of 1.5 μm), 100 μl of a stock solution of Nile red (0.057 mg/ml in methylene chloride) were added to the methylene chloride phase prior to emulsification [12].

All capsules were prepared freshly and were used the same day for animal experiments.

3.2. Animal experiments

3.2.1. Animals

A total number of 60 male Wistar rats (Rattus norvegicus, 448 ± 23 g) were obtained from the central animal unit of the Essen University Hospital. Animals were kept under standardized conditions of temperature (22 ± 1 °C), humidity (55 ± 5%), and 12/12-h light/dark cycles with free access to food (ssniff-Spezialdiäten, Soest, Germany) and water. All animals received humane care according to the standards of Annex III of the directive 2010/63/EU of the European Parliament and of the Council of 22 September 2010 on the protection of animals used for scientific purposes [13]. The experimental protocol was approved by the local committee for animal protection based on the local animal protection act.

3.2.2. Anesthesia, analgesia, and surgical procedure

Rats were anesthetized with isoflurane (2.0% in 100% medical O2 at 4.0 l/min for induction, 1.5–2.0% isoflurane in 100% medical O2 at 1.0 l/min throughout the experiment) through face masks connected to a vaporizer (Isofluran Vet. Med. Vapor; Draeger, Luebeck, Germany) and received ketamine (50 mg/kg body weight) subcutaneously into the right chest wall for analgesia. After local lidocaine administration (5 mg/kg body weight subcutaneously), a median skin-deep inguinal incision of about 2 cm was made along the right groin and a Portex catheter (0.58 mm, 1%) was placed within the right femoral artery and the right femoral vein. Each catheter was made along the right groin and a Portex catheter (0.58 mm ID, 0.96 mm OD) was placed within the right femoral artery and the right femoral vein. At the end of experiment, animals were sacrificed by resection of the heart, liver, spleen, lung, kidney, brain, M. gastrocnemius and small intestine under deep isoflurane anesthesia.

3.2.3. Study groups

In the main setting we compared three experimental groups. One group (n = 14) received PFD-filled PLGA microcapsules (1.5 μm), one group (n = 9) was medicated with a sterile solution of 0.25% PVA (maximum possible concentration of PVA remainder from capsule synthesis) and one group (n = 9) was treated with 0.9% NaCl. All solutions were infused continuously for 30 min into the right femoral vein using a syringe pump (20 ml/kg body weight × h). The total volume of 20 ml/kg body weight was
was continuously monitored using a rectal sensor; cooling below 0.1°C/minute every 10 min. The core body temperature of the rats was determined by counting the ventilation movements. The breathing rate was determined from systolic blood pressure spikes. The breathing rate was determined from the femoral artery catheter that was connected to a pressure transducer and displayed on a monitor. Ringer solution was infused via the femoral artery (with the additional effect to keep the catheter functional). In order to obtain plasma, blood was centrifuged at 4000g for 15 min at room temperature. The gained plasma was stored at 4°C until use (maximal within 4 h).

3.2.5. Blood gas analysis. Arterial blood pH, oxygen and carbon dioxide partial pressures (pO₂, pCO₂), base excess (BE), bicarbonate and lactate were assessed with a blood gas analyzer (ABL 715, Radiometer, Copenhagen, Denmark).

3.2.5.2. Enzyme activities. The plasma activity of lactate dehydrogenase (LDH) as a general marker of cell injury, creatine kinase (CK) as a marker for muscle cell injury, aspartate aminotransferase (ASAT) and alanine aminotransferase (ALAT) as markers for hepatocyte injury as well as the plasma creatinine concentration as a marker of renal function were determined using a fully automated clinical chemistry analyzer (Vitalab Selectra E, VWR International, Darmstadt, Germany) using commercially available reagent kits (DiaSys, Holzheim, Germany).

3.2.6. Assessment of microcirculation and physiological functions

3.2.6.1. In vivo microscopy. In vivo microscopy analysis (IVM) was performed with a Leica DMLM epifluorescence microscope (Leica Microsystems, Wetzlar, Wetzlar, Germany, x 160 magnification). Anesthesia Analgesia, and surgical procedures were the same as in the setting without IVM. The left lateral liver lobe was exteriorized on a specially designed stage 40 min after catheterization of the femoral vessels. The abdominal cavity was kept moist. One milliliter/kilogram body weight of fluorescein isothiocyanate-dextran 150,000 (FITC-dextran, 5% solution in 0.9% NaCl) was injected intravenously for fluorescent staining of liver microcapillaries [17]. Fifteen min after application of FITC-dextran, PLD-filled PLGA microcapsules (either 1.5 or 1 μm), PLGA microspheres (1.5 μm) or 0.9% NaCl solution were infused continuously for 30 min into the right femoral vein using a syringe pump (20 ml/kg body weight x h). During the measurement, animals were biomonitored continuously as described.

The following parameters were determined in five randomly selected acinar areas and postsinusoidal venules:

1. Diameters of sinusoids and postsinusoidal venules by an image analysis software (Kappa ImageBase 2.8.2.11051, Kappa Optronics GmbH, Gleichen, Germany).

2. The number of perfused vessels (the ratio of perfused sinusoids to all sinusoids visible in a defined acinar area) (%) by analyzing full video sequences by an examiner blinded to the experimental groups.

3.2.6.2. Frozen section procedure. In order to evaluate the in vivo distribution of PLD-filled PLGA microcapsules, cryosections of liver, spleen, lung, kidney, brain, heart and M. Gastrocnemius were prepared. Anesthesia, analgesia, and surgical procedures were the

chosen, because this is a typical volume (5-30 ml/kg body weight) for studies with oxygen carriers [2,14]. The short infusion time of 30 min was selected as pre-hospital treatment of trauma or other severely injured patients (the potential target population for artificial oxygen carriers) should not exceed 30-40 min [15,16]. After the stop of infusion, 12 animals were monitored for 4 h. As high blood volumes were required for determination of cytokines and complement factors, for 20 animals the main setting was shortened from 270 to 150 min and 90 min, respectively (NaCl and PFD-filled PLGA microcapsules (1.5 μm n = 4 for both time points).

The frozen section procedure (see below) was performed in an additional setting only slightly differing from the main setting (see section frozen section procedure) with 2 groups, one receiving 1 μm PFD-filled PLGA microcapsules (n = 2) and one receiving 1.5 μm PFD-filled PLGA microcapsules (n = 2).

For the assessment of hepatic microcirculation, in vivo microscopy (intravitral microscopy, IVM) was performed in an independent setting (see section in vivo microscopy) with 4 groups: PFD-filled PLGA microcapsules (1 and 1.5 μm), PLGA microspheres (1.5 μm) and 0.9% NaCl each n = 6.

3.2.4. Biomonitring

Systolic blood pressure, diastolic blood pressure and mean arterial blood pressure (MAP) were recorded continuously via the femoral artery catheter that was connected to a pressure transducer and displayed on a monitor. Ringer solution was delivered at 3 ml/h to keep the catheter functional. Heart rates were determined from systolic blood pressure spikes. The breathing rate was determined by counting the ventilation movements per minute every 10 min. The core body temperature of the rats was continuously monitored using a rectal sensor; cooling below 37°C was prevented by both an underlying thermostat-controlled operating table and by covering the animals with aluminum foil.

3.2.5. Assessment of blood and plasma parameters

Blood samples (0.5 ml) for both blood gas analysis and the monitoring of released enzymes activities in plasma in the main setting (see study groups) were taken from the femoral artery catheter before the start of infusion (after catheterization of A. femoralis) and subsequently 90, 150, 210 and 270 min after start of the infusion using a 2 ml syringe containing 80 IU electrolyte-balanced heparin (Picso50, Radiometer Medical, Brønshøj, Denmark). Inflammation parameters were determined only at the end of experiment in each setting at 90 min, 150 min or 270 min. For each blood sampling animals were substituted with a 0.5 ml bolus of 0.9% NaCl via the femoral artery (with the additional effect to keep the catheter functional). In order to obtain plasma, blood was centrifuged at 4000g for 15 min at room temperature. The gained plasma was stored at 4°C until use (maximal within 4 h).

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3.2.5.3. Inflammation parameters. The plasma concentration of the cytokines Interferon-gamma (IFN-γ), Interleukin-1alpha (IL-1α), IL-1β, IL-4, IL-5, IL-6, IL-10 and tumor necrosis factor alpha (TNF-α) were determined by using a rat-specific multiplex bead suspension array (Bio-Plex Cytokine Assay) in conjunction with a Bio-Plex Array Reader (Bio-Rad, Muenchen, Germany).

The plasma concentration of complement factors 3 (C3) and 4a (C4a) were assessed with rat-specific ELISA kits (Rat complement fragment 4a ELISA kit, Cusabio, Wuhan, China, and Rat Complement Factor 3, GenWay Biotech Inc, San Diego, CA, USA) according to the manufacturer’s instructions.

3.2.6. Assessment of microcirculation and physiological functions

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same as in the setting without frozen section procedure. Fluorescent-stained microcapsules (1.5 μm) were infused continuously for 30 min into the right femoral vein using a syringe pump (20 ml/kg body weight) 30 min after catheterization of the femoral vessels. Microcapsules were allowed to circulate for 40 min. Afterwards the organs were cryopreserved and frozen. Cryosections of spleen (A), liver (B) and lung (C) were prepared and nuclei were stained with DAPI (blue) for fluorescence microscopic analysis (×200 magnification). For assessment of the effect of capsule infusion on tissue damage, unstained PFD-filled PLGA microcapsules (1.5 μm) were infused for 30 min (20 ml/kg body weight × h). Microscopic assessment (×100 magnification) of spleen (D), liver (E) and lung tissue (F).

3.2.7. **Histological evaluation of the spleen, liver, lung and small intestine**

For histological examinations liver, spleen, small intestine and lung were resected. Subsequent to its resection, the small intestine

![Image](image-url)
was immediately cut into 10 pieces of equal length (9.5–10.5 cm). The median liver lobe, the spleen and the forth segment of the small intestine (serially numbered from jejunum to ileum) were fixed in formalin (10% neutral buffered) for 24–48 h. Before the thorax was opened, the lung was filled with 5 cm³ air via a canula after tracheotomy, then harvested, filled with formalin (5 ml) to ensure complete unfolding and finally submersed in formalin, as the other organs. Paraffin-embedded sections were stained with hematoxylin and eosin and evaluated in a blinded manner. Histological changes in the small intestine were scored on a scale from 0 to 8 (adaptation of the Park/Chiu system [18,19]). Using light microscopy, spleen sections (×100 and ×400 magnification) were assessed for integrity of red and white pulp, lung sections (×100 and ×400 magnification) were scanned for swelling of alveolar walls caused by bleeding or accumulation of water into the tissue and alveolar walls, liver sections (×100 and ×400 magnification) were investigated for disruption of parenchyma and vacuoles using the AxioVision Rel. 4.6 software (Zeiss, Jena, Germany).

3.3. Statistics

Biochemical assays were run in duplicate unless stated otherwise. Data are expressed as mean values ± SEM. Comparisons among multiple groups were performed with one-way analysis of variance (ANOVA) either for nonrecurring or for repeated measures followed by Dunnett (Figs. 1, 3, S1, S2, S4 and S6) or Sidak (Fig. 4) post-hoc analysis by using the graph pad prism 6.02 software (GraphPad Software, La Jolla, USA). Only data presented in the supporting information Fig. S5 was analyzed with two-way ANOVA followed by Dunnett post-hoc analysis. A p-value < 0.05 was considered to indicate significance.

4. Results

4.1. Systemic reactions

4.1.1. Hemodynamics and other systemic parameters

MAP in the NaCl control group remained in the physiological range (90–120 mmHg) throughout the whole experiment (Fig. 1). MAP in the PVA group differed only slightly from control (91–100 mmHg). In sharp contrast, animals receiving PFD-filled PLGA microcapsules with a diameter of 1.5 μm experienced a significant, temporary descent of MAP to 57 mmHg shortly after start of infusion, regaining baseline conditions after about 70 min. In all three groups heart rates stayed constant at about 300 bpm (Fig. S1A). In the PVA and microcapsule groups breathing rates increased from baseline level (about 50 breaths per min) to about 60 breaths per min from 0 to 80 min normalizing afterwards to baseline level (Fig. S1B). The body temperature of all animals was inconspicuous and persisted around 37 °C (Fig. S1C).

4.1.2. Acid–base and metabolic status

The pH of all animals was slightly acidic at about 7.3 (Fig. S2A), pCO₂ was mildly elevated to about 55 mmHg (Fig. S2B) while pO₂ was inconspicuous and varied around 500 mmHg in all three experimental groups (Fig. S1D). Base excess diminished somewhat in the NaCl and PVA treated animals, but did not move out of the physiological range (+3 to –3 mmol/l, Fig. S2C). However, the animals treated with microcapsules suffered from a significant decline from −0.9 mmol/l (0 min) to −5.9 mmol/l (120 min), compared to NaCl-infused animals. Blood lactate concentration in the NaCl and PVA groups increased only slightly to 1.2 and 1.0 mmol/l, respectively (Fig. S2D). In contrast, in the animals treated with microcapsules, lactate concentration significantly increased. Values doubled from 0.8 mmol/l (0 min) to 1.7 mmol/l (120 min) finally descending to control level at the end of the experiment (Fig. S2D).

4.2. Organ distribution and organ/tissue damage

Assessment of cryosections revealed an excessive accumulation of PFD-filled PLGA microcapsules (1.5 μm) in spleen and liver (Fig. 2A–B) but displayed very few capsules in other organs, i.e., lung (Fig. 2C), brain, kidney, heart and M. Gastrocnemius (Fig. S3). Identical results were obtained after infusion of 1 μm-sized PFD-filled PLGA microcapsules (data not shown).

Infusion of NaCl or PVA did not affect plasma activities of the enzymes ALAT, ASAT, CK and LDH (Fig. 3). In contrast, after infusion of PFD-filled PLGA microcapsules plasma activities of ALAT (3.6-fold), ASAT (6-fold), CK (5-fold) and LDH (24-fold) were significantly elevated if compared to the NaCl group at the end of experiment (Fig. 3). Creatinine concentrations oscillated around 0.7 mg/dl in all three experimental groups (Fig. S4).

Hematoxylin-eosin-staining revealed changes of spleen and liver architecture. Compared with NaCl- or PVA-infused animals (free of pathological indications), spleens of animals treated with PFD-filled PLGA microcapsules showed beginnings of dissolving tissue structures of white pulp and red pulp (Fig. 2D). Liver structures were still distinguishable but offered some vacuoles (Fig. 2E), while lung tissue was intact and did not display any sign of thickened alveoli walls (Fig. 2F).

Microscopic investigations of the mucosa of the fourth segment of the small intestine did not reveal distinct pathological changes in any group (data not shown). In contrast, in the group of animals treated with PFD-filled PLGA microcapsules macroscopic assessment of the serosa revealed some petechiae scattered over the entire jejenum.

4.3. Effects on inflammation parameters

Plasma concentrations of IL-1α, IL-1β, IL-6, IL-10 and TNF-α displayed similar characteristics. After the infusion of PFD-filled PLGA microcapsules, pro-inflammatory cytokines (such as IL-1α, IL-1β, IL-6, TNF-α) were strongly elevated compared to NaCl controls, whereas infusion of PVA did not provoke any immune response (Fig. 4A–H). Notably, 90 min after begin of microcapsule infusion a clear increase of IL-10 took place and persisted until the end of the experiment (Fig. 4I). Irrespective of the treatment group, plasma levels of both IL-4 (<141.4 pg/ml) and IFN-γ (<35.0 pg/ml) were unaffected and only very small amounts of IL-5 (<113.0 pg/ml, not significantly different between the treatment groups) were released (Fig. 4C/D/G).

The application of NaCl did not alter the concentration of complement factor 3 (C3) in plasma. Only at 270 min, C3 level in the group treated with PFD-filled PLGA microcapsules was significantly different between the treatment groups (Fig. 4J). Infusion of NaCl or PVA did not affect the plasma amount of complement factor 3a (C3a) either. In both groups all values stayed below the assay’s detection limit (Fig. 4J).

4.4. Effects on microcirculation

The diameters of sinusoids and postsinusoidal venules increased about 23% and 20% already 10 min after start of infusion of PFD-filled PLGA microcapsules (1.5 μm and 1 μm, respectively) whereas infusion of PLGA microshpere caused a decrease of vessel diameter of 15% compared to NaCl control group (Fig. S5).
During the following 20 min of infusion, diameters of sinusoids and postsinusoidal venules of all microcapsule treated animals normalized, thereby reaching the baseline level at the end of the infusion (Fig. S5).

After infusing 0.9% NaCl, the number of perfused vessels and MAP remained at baseline levels (100%, 100 mmHg, respectively, Fig. 5A). In contrast, at the very beginning of the infusion of PFD-filled PLGA microcapsules (1.5 μm) MAP (mmHg) and the number of perfused vessels (%) decreased to about 60 mmHg/50% from baseline. Only MAP regenerated during the following observation time, whereas the number of perfused vessels only reached 80% of baseline level (Fig. 5B). Infusion of PFD-filled PLGA microcapsules (diameter 1 μm) revealed identical results as obtained with 1.5 μm microcapsules (Fig. S6). After treatment with PLGA microspheres MAP did not decrease but stayed in the physiological range (85–100 mmHg) throughout the whole experiment (similar to the NaCl group) and the number of perfused vessels slowly decreased leveling off at 80% of baseline level after 150 min (Fig. 5C).

5. Discussion

5.1. Study rationale

Blood losses up to a hemoglobin level of 10 g/dl are generally well tolerated by patients. Intervention with red blood cell concentrates or artificial oxygen carriers becomes necessary when hemoglobin level would further decrease. If and how many red blood cell concentrates are transfused (in default of approved artificial oxygen carriers) not only depends on the individual patient’s condition but also on the hospital’s practice, whereas at a hemoglobin decrease below 6 g/dl transfusion of red blood cell concentrates is generally indicated [20]. If transfusion is inalienable, until now, usually 2 or more red blood cell concentrates are required, as the average increase in hemoglobin level per unit red blood cell concentrate is only 1.0 g/dl [21]. Therefore, the tolerance of high quantities of foreign particles in the intravascular system is a prerequisite for the successful use of microcapsules as artificial oxygen carriers and implies both, the occurrence and the monitoring of new toxicity profiles. So far the infusion of 1247 mg PFD-filled PLGA microcapsules/kg body weight is clearly higher than common dosing of intravenously administered polymeric pharmaceuticals (ca. 23 mg/kg body weight [7], 440 mg/kg body weight [22]). Not only quantitatively but also in relation to the blood volume the amount of infused microcapsules is high (1/6 of the blood volume, assuming the calculation of the rat’s blood volume proposed by Lee et al. [23]), which is in the same order of magnitude as demonstrated for PLA90 nanoparticles (also 1/6 [22] but much higher than similar-sized microparticles [1/28] [7] or ultrasound contrast agents [1/20,000] [8]. Assuming a mean blood volume of 4–6 l for humans, 1/6 (0.67–1.0 l) corresponds to 2.4–3.6 red blood cell concentrates (0.28 l).
Fig. 4. Effect of capsule infusion on release of cytokines and complement factors. PFD-filled PLGA microcapsules (1.5 μm), 0.25% PVA or 0.9% NaCl were infused for 30 min (20 ml/kg body weight × h). The values plotted are mean ± SEM of 6-4 (capsules) or 3 (PVA and NaCl) individual experiments, *p < 0.05 compared to NaCl group. The detection limit of the used ELISA was 0.08 ng/ml. Note: logarithmic scale was used for Fig. 4E, F and H. C4a level in NaCl and PVA groups at all time-points measured were below detection limit.
5.2. Effects on MAP

Transient systemic hypotension after infusion of PFC-based artificial oxygen carriers has been described long ago for PFC-based emulsion systems [24,25] and latterly also for capsule-based PFC-containing systems [26]. This undesirable side effect has been attributed to the action of the emulsifier without [27,28] or in combination with the PFC [29]. In order to safely exclude any emulsifier-caused side effects, a control group receiving PVA only (without microcapsules) was implemented, although the short-chained PVA used in this study is known as biocompatible and eliminable [27,28]. The results of our experiments (Fig. 1, our results are comparable to the data of Ingram et al., suggesting, that only the combined action of PFC and emulsifier is responsible for transient hypotension [29]. Furthermore, hypotension only occurred after application of PFD-filled PLGA microcapsules (Fig. 1, Fig. S2) but not after application of PFD-free PLGA microspheres (Fig. 5C). Due to the fact that transient hypotension was also described after intravenous application of PFD-filled poly(β-butyl-cyanoacrylate) nanocapsules [26], transient hypotension may be a general complication of perfluorocarbon-based products irrespective of the type of galenic packaging (emulsion or capsule) of the oxygen carrier.

The proposed mechanism for this transient hypotension would be the prompt activation of the complement system leading to the release of vasoactive substances [28,29,32,33]. As anaphylatoxins can regulate vasodilation and increase permeability of small blood vessels [34,35], a decline of C3 concentration in plasma and increase of the anaphylatoxin C4a after infusion of microcapsules (but no changes after treatment with PVA) are in line with this hypothesis (Fig. 4I,J). Activation of both, the classical and the alternative pathway of the complement system are possible by contact of blood with artificial particles [36,37]. The clear increase of C4a (not part of the alternative pathway [38,39]), should support an involvement of the classical pathway. Activation of the classical pathway (initiated by the adsorption of plasma proteins such as IgG and albumin) can also amplify the alternative pathway mediating primarily the reaction against foreign biomaterials [40]. Since PEG-shielding can only partly reduce protein adsorption on surfaces of PLGA particles [5,37], adsorbed IgG may mediate activation and binding of C3b to the capsules’ surface as proposed by Nilsson et al. [38]. A complement activation-related pseudoallergy (CARPA) that is already confirmed for different nanoparticles, polymers and emulsifiers such as Cremophor EL or Tween [41,42] was not responsible for transient hypotension (Figs. S1 and S2). Even though in contradiction to CARPA symptoms in pigs and dogs [41,43] this is not surprising, as rats are especially insensitive to CARPA [44].

Another explanation for transient hypotension would be an involvement of nitric oxide-mediated (NO) pathways. Short- and long-term regulation of NO production in response to shear stress on the endothelial membrane of vasculature (as potentially caused by the heavy-weight PFD-filled microcapsules) is well-known [45,46]. Additionally, the formation of relatively stable S-nitrosothiols (believed to act as biological metabolites and carriers of NO) in the blood in presence of perfluorocarbons (as PFD) can induce NO release via synthesis of intermediates, that are highly effective in nitrosating other compounds [47–49]. This process can also be triggered by shear force on endothelial cells [50].

However, an effect on MAP evoked primarily by the release of cytokines seems unlikely, although release of cytokines from monocytes, macrophages and lymphocytes after contact with PLGA is described in vitro and in vivo [51–54]. The cytokine profile after infusion of PFD-filled PLGA microcapsules (Fig. 4A–H) is in line with in vitro data from mononuclear cells cultured in the presence of poly-(l-lactide) [52] and macrophages cultured in the presence of PLGA microparticles [diameter of 6.5 μm] [53]. The strong release of IL-10 may counteract the effects induced by the pro-inflammatory cytokines, avoiding an excessive immune response by, among others, influencing production of TNF-α [51,52]. Nevertheless a direct relation between release of cytokines and transient hypotension cannot be propagated, as cytokine levels in plasma remained elevated until the end of the experiment (Fig. 4A–H), whereas MAP normalized after 70 min (Fig. 1, Fig. 5B). Likewise, the reported appearance of allergic and anaphylactic reactions to some PFC-containing emulsions [9] leading to hypotension cannot be used as an argument in the present study as the IL-5 level obtained after application of PLGA microcapsules did not differ significantly from corresponding NaCl control values (Fig. 4D).

5.3. Effect on microcirculation and distribution pattern

Hepatic sinusoidal blood flow depends among other factors on MAP and sinusoidal diameter, whereupon reduced sinusoid diameter causes impairment of sinusoidal blood flow [55]. Decreased number of perfused vessels is certainly mostly entailed by the prompt and radical drop of MAP after application of PFD-filled PLGA microcapsules (Fig. 5B), because undesirable artifacts due to
5.4. Effects on acid–base metabolism and tissue oxygenation

Persisting microcirculatory impairment can lead to tissue hypoxia and the development of subsequent organ dysfunction [55]. Thus, the function of oxygen carriers is to improve the microcirculation as already established for a PFC-based emulsion and a hemoglobin-based suspension [55,59]. However, animals treated with PFD-filled PLGA microcapsules experienced a mild metabolic acidosis (Fig. S2) corresponding to the data of Sedova et al. describing the same phenomenon after infusion of a PFC-containing emulsion [60].

Probable lactate formation in muscle tissue increases due to transient hypotension and reduced number of perfused vessels of sinusoids. This can entail an undersupply of affected tissue areas with oxygen triggering anaerobic glycolysis [61]. The increase in enzyme activities in plasma, such as LDH as a general marker of cell injury and CK as a marker for muscle cell injury, should further support the assumption of cellular damage (Fig. 3C and D). An increased LDH level was also described after contact of silica microparticles with human endothelial cells and after pulmonary exposition of rats to polystyrene particles [62]. In contrast, intravenous injection of nanoporous silicon dioxide particles [57] and 2 μm-sized silicon dioxide particles [57]. While other investigators additionally observed an accumulation of microparticles in lung tissue [57,58], our results showed neither enrichment in that organ nor swollen alveolar walls (Fig. 2C and F).

6. Conclusions

Generally, the infusion of high quantities of PFD-filled PLGA microcapsules was tolerated as all animals survived the selected observation period. Nevertheless, the findings of this study imply a new toxicity profile compromised with severe side effects that are only partially described for other intravenously infused foreign particles and for the used materials such as PFD so far. As expected from previous studies about the pharmacokinetics and biodisposition of different PVA [30,31], in the present investigation, short-chained PVA was completely harmless in vivo during an observation time of 4 h.

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Appendix A. Supplementary Material

Supplementary material associated with this article can be found, in the online version, at http://dx.doi.org/10.1016/j.rinphs.2014.04.001.

References


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